

INTRODUCTION

Most cochlear-implant (CI) signal-processing strategies are based on Continuous Interleaved Sampling (CIS), which band-pass filters the input signal and extracts its envelope at the filter output, which is then used to modulate the amplitude of a fixed-rate pulse train (Fig. 1C). As such, **CIS largely discards temporal fine structure (TFS) information**⁽¹⁾.

To convey the TFS of incoming signals, MED-EL's **Fine Structure Processing (FSP) strategy**⁽²⁾ detects the positive zero-crossings in the band-pass filter output (Fig. 1A), which then triggers a short burst of pulses (Fig. 1B) to the 4 most apical electrodes (e1-e4).

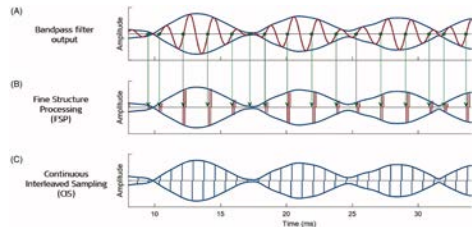


Fig. 1. Stimulation with the FSP strategy at the apical electrodes (A-B). CIS is applied to all other electrodes (C). Figure courtesy of Dhanasingh and Hochmair (2021).

For the FSP strategy to work:

- I. **Temporal pitch perception should be accurate at the apex of the cochlea (Exp. I)**
- II. **The pitch of a harmonically-related multi-electrode stimulus should be (Exp. II):**
 - Equal to its fundamental frequency (F_0)
 - Unaffected by inter-channel interactions

EXPERIMENT I

METHOD:

Participants: 8 experienced MED-EL users

Procedure:

- **Place-pitch ranking** of e1 to e4 using the midpoint comparison (MPC) procedure⁽³⁾
- **Rate-pitch ranking** of 8 pulse rates (80-981 pps) using the MPC procedure for:
 - (i) single-electrode apical (e1) stimulation
 - (ii) single-electrode mid (e8) stimulation
 - (iii) simultaneous multi-electrode apical (e1-e4) stimulation
- Neural health measured at e1 and e8 by the **polarity effect (PE)** = detection threshold difference between 99-pps triphasic pulses with cathodic (TP-C) vs. anodic (TP-A) dominant polarity⁽⁵⁾

RESULTS:

- 4/8 patients demonstrated apical (e1/e2) place-pitch confusions
- The upper limit of temporal pitch did not differ between the 3 stimulation conditions (Fig. 2)
- Rate-pitch ranking was not correlated to place-pitch ranking or the PE

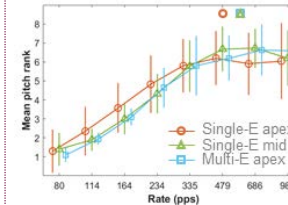


Fig. 2. Mean rate-pitch ranks and SD as a function of pulse rate and stimulation condition. Coloured shapes at the top of the graph indicate the upper limit estimates.

EXPERIMENT II

METHOD:

Participants: 8 experienced MED-EL users

Procedure: **Rate-pitch ranking** of 11 multi-electrode stimuli (Fig. 3), presented to e1-e4 and including a simple approximation of the FSP strategy ([1234]xSD, shown by box), using the MPC procedure

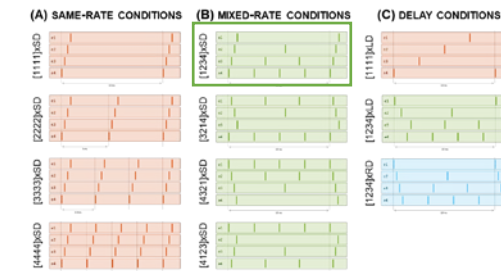


Fig. 3. Visualisation of 10 ms of the 11 multi-electrode stimuli used in Experiment II. [numbers]*100 refer to the rate that was applied to e1-e4. SD = 100- μ s Short Delay; LD = maximised Long Delay; RD = Reversed Delay.

RESULTS:

- The pitches of harmonically-related mixed-rate stimuli were ranked between 100 and 200 pps (Fig. 4)
- Maximising the inter-electrode delay (SD vs. LD) increased the pitch of both same- and mixed-rate stimuli
- Stimulation order (SD vs. RD) did not affect the pitch rank

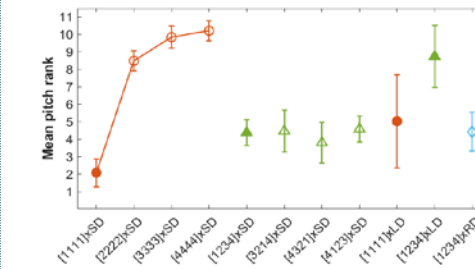


Fig. 4. Mean rate-pitch ranks and SD as a function of stimulation condition.

DISCUSSION

I. **There is no justification for conveying TFS cues specifically or exclusively to the apical electrodes** in order to increase the upper limit of temporal pitch - in line with earlier studies⁽⁵⁾.

II. **There is no evidence that presenting multiple harmonically-related rates to different apical electrodes elicits a pitch percept at F_0 .** In addition, the pitch was affected by between-channel interactions.

Additional findings (not shown): (i) the PE correlated with the average threshold and (ii) the PE did not differ between apical and mid-array stimulation, contrary to some model predictions⁽⁶⁾.

Practical implications: Strategies that deliver a different temporal code to each electrode are likely to elicit a complex pattern of auditory-nerve responses as a result of spread of excitation, which might additionally vary with frequency-dependent phase distortions (e.g., due to reverberation⁽⁷⁾).

- (1) Wouters, J., et al. (2015). IEEE Signal Process. Mag., 32(2), 67-80
- (2) Dhanasingh, A., & Hochmair, I. (2021). Acta Otolaryngol., 141(Sup 1), 106-134
- (3) Long, C. J., et al. (2005). Ear Hear., 26(3), 251-262
- (4) Mesnildrey, Q., et al. (2020). JARO, 21, 89-104
- (5) Kong, Y. Y., & Carlyon, R. P. (2010). JASA, 127(5), 3114-3123
- (6) Kalkman, R. K., et al. (2014). Ear Hear. 315, 10-24
- (7) Sayles, M., & Winter, I. M. (2008). Neuron 58(5), 789-801